

## ELECTROSYNTHESIS OF Cu / ZnO NANOCOMPOSITE ELECTRODE ON ITO ELECTRODE AND ITS APPLICATION IN OXIDATION OF ASCORBIC ACID AND GLUCOSE

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### Abstract

In the present study Cu nanoparticles (NPs), ZnO nanorods have been deposited on indium tin oxide (ITO) electrode and thereby Cu-NPs /ZnO / ITO composite film electrode has been prepared. The prepared nanostructures have been characterized by using scanning electron microscope (SEM). The shape of the electrochemically deposited ZnO follow rod like structure on ITO electrode, Cu-NPs follow irregular spherical shape when electrodeposited on ITO electrode. Oxidation of ascorbic acid on bare ITO electrode is favorable than that of ZnO modified ITO electrode but Cu-NPs/ ZnO composite electrode had high sensitivity and stability and showed higher catalytic current for glucose oxidation.

Key words: Nanoparticles (NPs), Nanocomposite electrode, Indium tin oxide (ITO), Ascorbic acid, Glucose

### Introduction

Electrochemical sensors and biosensors for the electroanalysis of biologically active compounds have attracted a great deal of interest due to their analytical performances (Xu *et al.* 2006). Electrochemical sensors provide low detection limits, a wide linear response range, and good stability and reproducibility, among other advantages (Zhang *et al.* 1997 and Chen *et al.* 2008). However, bare electrodes are more likely than chemically modified electrodes to suffer from interferences or surface fouling by products arising from follow-up reactions, associated to the main electrochemical process. The modification of electrode surfaces with inorganic or organic coatings often avoids these drawbacks and represents a rapid and versatile resource for the preparation of stable and selective new electrochemical sensors (Evans *et al.* 2004 and Wang 2008).

Electrochemical methods have potential application in the detection of D (+)-glucose in blood samples (Wilson and Turner 1992) and also in bio-fuel cells (Park *et al.* 2006). Glucose oxidase (GOD) is one of the most extensively studied enzyme and has been successfully employed for preparing glucose biosensors. The development of glucose biosensors utilizing GOD is an active research area (Chen *et al.* 2002, Evans *et al.* 2004 and Wang 2008). A majority of glucose sensors, especially those used in in-vivo application are based on the electrochemical oxidation of hydrogen peroxide which is formed in the course of the enzyme-catalyzed oxidation of glucose by dissolved oxygen.

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Recently, excellent review articles have been published and discussed about the principles of electrochemical glucose biosensors and key challenges in their further development and use. It is shown that nano-ZnO film provides better environment and enhanced electron transfer between ChOx and electrode (Lupo *et al.* 2010).

Over the past decades, a number of studies have been conducted to alleviate the drawbacks of enzymatic glucose sensors. The most common and serious problem is insufficient stability originated from the nature of the enzymes which is hardly overcome. Although glucose oxidase (GOD) is quite stable compared with other enzymes, the glucose sensors based on GOD are always exposed to the possible thermal and chemical deformation during fabrication, storage or use. Further, GOD quickly loses its activity below pH 2 and above pH 8 and temperature above 40 °C can cause fatal damages (Wilson and Turner 1992). Ionic detergents also deactivate GOD as well. To overcome the above obstacles, non-enzymatic glucose sensors have been developed and kept coming closer to practical applications. Park and coworkers discussed about the merits and mechanism of glucose oxidation on non-enzymatic sensors (Park *et al.* 2006). Nanostructured particles have attracted extensive scientific and industrial interest due to their unique electronic, optical and catalytic properties. Nanoparticles can display four unique advantages over microelectrodes when used for electro analysis. These are: enhancement of mass transport, catalysis, high effective surface area and control over electrode microenvironment (Lupo *et al.* 2010). Electrochemical deposition of copper nanoparticles (Cu-NPs) and their applications in electro-catalysis is an active research area (Miao *et al.* 2008). Though, the Cu-NPs were prepared in several matrixes by several researchers, no effort has been made to prepare Cu-NPs embedded in functional matrix material like zinc oxide (ZnO). In our laboratory zinc oxide (ZnO) nano particles have been prepared by using simple combustion methods and by electrochemical methods onto ITO electrode in order to use as nano-electrodes. In the present study, ZnO NPs were deposited on the ITO electrodes by electrochemical method. Copper NPs were deposited onto ZnO/ITO electrode to obtain Cu-NPs / ZnO /ITO composite film electrode using electrochemical technique. The characterization of these electrodes have been performed by using SEM and possible applications of these electrodes as sensors have been examined by using electrochemical methods.

### Materials and Methods

This research work was carried out at the physical chemistry research laboratory, Dhaka University, during the period of 2010.

Chemicals: Potassium chloride, KCl (BDH, UK), zinc nitrate,  $Zn(NO_3)_2 \cdot 6H_2O$  (MERCK, India), zinc acetate,  $Zn(CH_3COO)_2 \cdot 2H_2O$  (MERCK, Germany), copper sulfate,  $CuSO_4 \cdot 5H_2O$  (MERCK, Germany), absolute ethyl alcohol, (AR, BDH), ethylene glycol (AR, BDH), sodium hydroxide, NaOH (AR, BDH),  $N_2$ , 99.99% pure (BOC, Bangladesh), sulfuric acid,  $H_2SO_4$  (AR, BDH), potassium per chlorate,  $KClO_4$  (AR, BDH), Glucose,

C<sub>6</sub>H<sub>12</sub>O<sub>6</sub> (AR, BDH), cetyltrimethyl ammonium bromide (CTAB) (BDH, UK), ascorbic acid, (C<sub>6</sub>H<sub>8</sub>O<sub>6</sub>), (Merck, Germany) and potassium ferricyanide, K<sub>3</sub>Fe(CN)<sub>6</sub> (Merck, Germany) were used without further purification.

Instruments: A Computerized Electrochemistry system, Model HQ 2040 was used in the present study. A pyrex glass volumetric cell (10 mL) with three electrode configurations, ITO as working electrode (area 3.2cm<sup>2</sup>), platinum wire as the counter electrode and Ag/AgCl (satd. KCl) as the reference electrode was used in this study.

SEM (Hitachi, S-3400, Japan) was used in this experiment. In this SEM accelerating voltage was fixed ranging from 0.3 kV to 30.0 kV. Resolution was set in 3.0 nm at 30.0 kV accelerating voltage in high vacuum mode for Secondary Electron (SE) image. Back Scattered Electron (BSE) image resolution was set in 4.0 nm at 30.0 kV accelerating voltage in low vacuum mode. For all these images magnification was set at a range 5 times to 300000 times. From this SEM image size and different shapes of nanoparticles were characterized.

Supporting electrolyte solution:

- (a) 100 mL of 0.1M KCl solution was prepared in deionized water.
- (b) 100 mL of 0.1M NaOH solution was prepared in deionized water.
- (c) CuSO<sub>4</sub>.5H<sub>2</sub>O solution: 10 mL of 0.1M Cu<sup>2+</sup> stock solution was prepared in 0.1M KCl.
- (d) K<sub>3</sub>Fe (CN)<sub>6</sub> solution: 10 mL of 0.1M K<sub>3</sub>Fe(CN)<sub>6</sub> solution was prepared in 0.1M KCl.
- (e) Glucose solution: 10 mL of glucose solution was prepared in 0.1M NaOH.
- (f) Ascorbic acid solution: 10 mL of 0.1M Ascorbic acid stock solution was prepared in 0.1M KCl.

Electrochemical Method for the preparation of ZnO NPs: The conventional three electrode cell in which ZnO NPs were prepared was maintained at 40<sup>0</sup>C in a water bath. The working electrode was a commercial ITO glass (30×66.66×6 mm, R(s) < 10 ohm). An aqueous solution of 0.1 M Zn (NO<sub>3</sub>)<sub>2</sub> mixed with 0.1 M KCl was used and deposition was carried out for an hour. ZnO nanoparticles were electrodeposited on ITO electrode at -1.1 V vs. Ag/AgCl reference electrode and a Pt electrode was used as counter electrode. After deposition the resulting nanodeposits were thoroughly rinsed with water and dried under a nitrogen atmosphere.

## Results and Discussion

Preparation of copper nanoparticles/zinc oxide composite modified electrode: ITO substrates were cleaned by using detergent, diluted hydrochloric acid and then finally rinsed with distilled water. Transparent ZnO films have been cathodically deposited onto conductive ITO glasses from a simple aqueous zinc nitrate electrolyte bath kept at 335 K. Electrodeposition of ZnO film was carried out potentiostatically (-0.7 V for 20 min)

using a potentiostat/galvanostat without stirring. ZnO-modified ITO was rinsed with distilled water to remove unbounded materials from the electrode surface and then dried by nitrogen gas. Cu-NPs were deposited onto a ZnO film coated ITO from the solutions of 0.01 M  $\text{CuSO}_4 + 0.1$  M  $\text{KClO}_4$  under fixed applied potential of  $-0.9$  V (vs. Ag/AgCl) for 3 min. For comparative studies, Cu-NPs were deposited onto an unmodified ITO as described above. Finally, the Cu-NPs/ZnO composite modified electrode was thoroughly washed with doubly distilled water to remove unbounded materials from the electrode surface and then dried in air for 30 min before use.

SEM images of ZnO nanoparticles: It is not possible to determine the exact particle size from SEM images which can be done through TEM analysis. The SEM images show the approximate concept about the formation of nanoparticles.

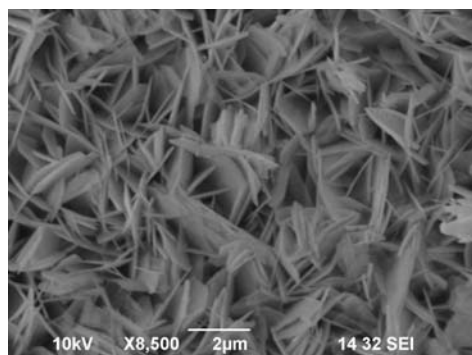


Fig. 1 (a) SEM image of ZnO NPs on ITO.

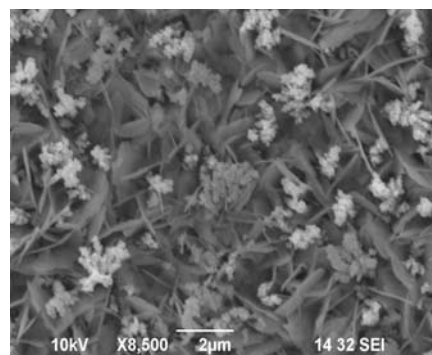


Fig. 1 (b) SEM image of Cu/ZnO NPs on ITO.

Fig. 1 shows the SEM images of (a) ZnO deposited on ITO electrode and (b) Cu particles formed on ZnO/ITO electrode. It is evident from above figures that ZnO NPs prepared by electrochemical methods on ITO electrode exhibit rod-like structures. ZnO NPs modified ITO electrode can be used as nanoelectrode. Cu NPs when deposited electrochemically on these modified electrodes follow irregular flower-like structures as shown in Fig. 1 (b). ZnO/ITO electrode and Cu NPs/ZnO/ITO composite film electrodes have been used in the present study as sensors.

Electrochemical behaviour of  $\text{K}_3\text{Fe}(\text{CN})_6$  on ITO electrode for different scan rates: Fig. 2 shows the CV of 0.40 mM  $\text{K}_3\text{Fe}(\text{CN})_6$  solution at different scan rates on ITO electrode. The potential was stepped from +0.650 V to a vertex potential of -0.150 V and finally the potential was reversed back to +0.650 V. The cathodic peak was observed at +0.158 V. The corresponding anodic peak was observed at +0.230 V. Both cathodic and anodic peak current increases with increasing scan rate and potential remain almost constant.

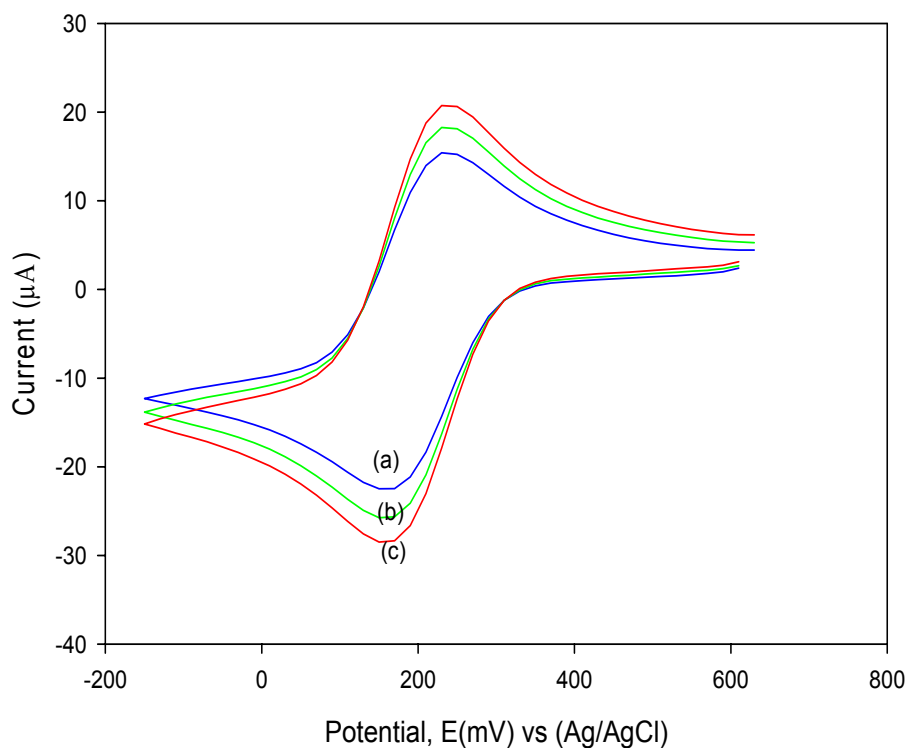


Fig. 2. CV of 0.40 mM  $K_3Fe(CN)_6$  solution at (a)  $15\text{ mVs}^{-1}$  (b)  $20\text{ mVs}^{-1}$  (c)  $25\text{ mVs}^{-1}$  S.R.

Electrochemical behaviour of  $K_3Fe(CN)_6$  on ZnO Modified ITO electrode for different scan rates : Fig. 3. Shows the CV of 0.40 mM  $K_3Fe(CN)_6$  solution at different scan rates on modified ITO electrode. The potential was stepped from +0.650 V to a vertex potential of -0.150 V and finally the potential was reversed back to +0.650 V. The cathodic peak was observed at +0.162 V. The corresponding anodic peak was observed at +0.245 V. Both cathodic and anodic peak current increases with increasing scan rate and potential remain almost constant.

Comparison of CV of  $K_3[Fe(CN)_6]$  solution between ITO electrode and ZnO modified ITO electrode : Here the CV of  $K_3[Fe(CN)_6]$  solutions (Fig. 4.) show that both the cathodic and anodic peak potential are almost at the same position for ITO electrode and modified ITO electrode.

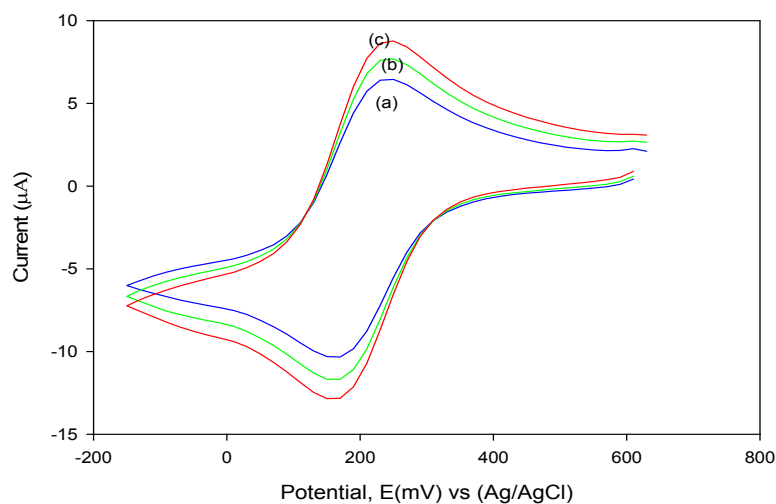


Fig.3. CV of 0.40 mM  $K_3Fe(CN)_6$  solution at (a)  $15\text{ mVs}^{-1}$  (b)  $20\text{ mVs}^{-1}$  (c)  $25\text{ mVs}^{-1}$  S.R.

But the current decreases significantly in the case of ZnO modified ITO electrode. The diffusion coefficient values were found as follows:

(a) The Diffusion co-efficient at ITO electrode  $=13.03 \times 10^{-8}\text{ cm}^2/\text{s}$

(b) The Diffusion co-efficient at ZnO modified ITO electrode  $=2.22 \times 10^{-8}\text{ cm}^2/\text{s}$ .

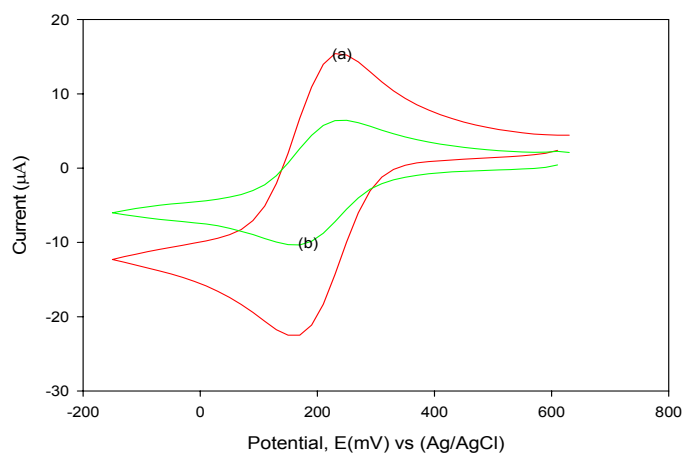


Fig.4. CV of 0.40 mM  $K_3[Fe(CN)_6]$  solution at (a) ITO electrode (b) ZnO modified ITO electrode at scan rate  $15\text{ mVs}^{-1}$ .

Oxidation of glucose on ITO, ZnO / ITO and Cu NPs/ ZnO / ITO composite electrode: From Fig. 5. it is evident that glucose exhibits an oxidation peak at around +0.8 V on ITO electrode (curve c) the peak current decreases when the CV is run on ZnO modified ITO electrode. However, the glucose oxidation enhances remarkably when the CV is carried out onto Cu NP/ ZnO/ ITO composite electrode. The peak current for glucose oxidation increases almost ten times indicating that Cu NPs play a strong catalytic role when deposited onto ZnO particles. CVs of the Cu NPs/ZnO composite modified electrode recorded in 0.1M NaOH in the presence (curve a) and absence (curve b) of 5 mM glucose. It exhibited a single oxidation peak around 0.4 to 0.8 V vs Ag/AgCl. Fig.5 (curve c and d) shows CVs obtained for glucose at a bare ITO electrode (curve c) and a ZnO modified electrode (curve d).

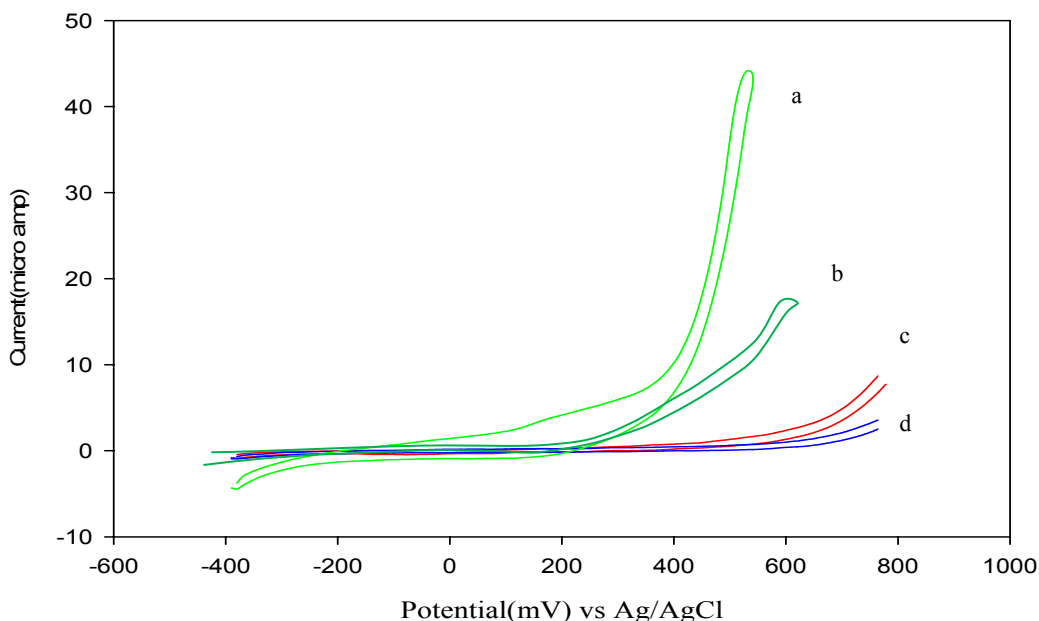


Fig. 5. The CVs of 5 mM glucose in 0.1 M NaOH solution at Cu-NPs/ZnO / ITO composite electrode (a) CV without glucose (curve b) The CVs of 5 mM glucose in 0.1 M NaOH solution at bare ITO (curve c) and at ZnO/ ITO (curve d) at a scan rate of  $20 \text{ mV s}^{-1}$ .

In this study ZnO nanostructures and Cu-NPs have been deposited onto ITO electrode by using electrochemical method. It was found that Cu-NPs / ZnO composite modified electrode exhibits higher electrocatalytic activity towards glucose oxidation. The obtained results revealed that determination of glucose can be easily performed using Cu-NPs/ZnO composite film electrode and the modified electrode enhanced the electrocatalytic activity remarkably towards glucose with high stability in its solution. The Cu-NPs, ZnO nanostructures and composite electrodes were characterized by SEM and CV. This method may open an avenue for electrochemical sensing of glucose, ascorbic acid, other

biomolecules and organic pollutants present in the environment. Further study for the development of non enzymatic electrochemical sensors is in progress.

### References

- Chen, X.H., Y.B. Hu and G.S. Wilson. 2002. Glucose microbiosensor based on alumina sol-gel matrix/electropolymerized composite membrane. *Biosens. Bioelectron.* **17** : 1005-1008.
- Chen, X., J. Chen, C. Deng, C. Xiao, Y. Yang, Z. Nie and S. Yao. 2008. Amperometric Glucose biosensor based on boron -doped carbon nanotubes modified electrode. *Talanta.* **76** : 763-768.
- Evans , R.G., C.E. Banks and R.G. Compton. 2004. Amperometric detection of glucose using self catalytic carbon paste electrode. *Analyst.* **129**: 428-433.
- Lupu, S., F. J. Del Campo and F. Xavier Muñoz. 2010. Development of microelectrodearrays modified with inorganic-organic composite materials for dopamine electroanalysis. *Electroanal. Chem.* **639**: 147-153.
- Miao, X.M. , R. Yuan, Y.Q. Chai, Y.T. Shi and Y.Y. Yuan. 2008. Direct electrocatalytic reduction of hydrogen peroxide based on nfin and copper oxide nanoparticles modified Pt electrode. *J. Electroanal. Chem.* **612** :157-162.
- Park, S., H. Boo and T.D. Chung. 2006. Electrochemical non-enzymatic glucose sensors. *Anal. Chim. Acta.* **556**: 46-52.
- Wang, J. 2008. In vivo glucose monitoring: Towards 'sense and act' feedback- loop individualized medical systems. *Talanta.* **75**: 636-642.
- Wang, J. 2008. Electrochemical Glucose Biosensors. *Chem. Rev.* **108**: 814-825.
- Wang, J., G. Chen, M. Wang and M.P. Chatrathi. 2004. Carbon nanotube / copper composite electrodes for electrophoresis microchip detection of carbohydrates. *Analyst.* **129** : 512-516.
- Wilson, R. and A.P.F. Turner. 1992. Glucose oxidase: an ideal enzyme. *Biosens. Bioelectron.* **7** : 165-169.
- Xu, Q. , Y. Zhao, J.Z. Xu and J.J. Zhu. 2006. Preparation of functionalized copper nanoparticles and fabrication of glucose sensor. *Sens. Actuators B.* **114**: 379-384.
- Zhang, X. , K.Y. Chan, J.K. You, Z.G. Lin and A.C.C. Tseung. 1997. Partial oxidation of glucose by a Pt / WO<sub>3</sub> electrode. *J. Electroanal. Chem.* **430**: 147-151.

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